

**Measured Accumulative Underlying Real-time ImpaCt Endo-skeleton  
“MAURICE”**

ECE4012 Senior Design Project

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**May 3, 2018**

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## Executive Summary

The main goal of our project is to design a tactile, mobile health monitor to be worn by football players at both college and professional levels. The motivation for designing such a product comes from the current issue revolving around repeated concussions, which increase players risk with health issues. This technology will notify the medical staff, not only that a player was injured, but also where they were hurt on the previous play. Despite precaution, players are sometimes moved hastily, causing further injury to the player as he may have not been able to indicate what bone or muscle was damaged. This suit will reduce the medical staff's dependence on the coherence of the player by using several sensors to monitor different parts of the body including, measuring the force of impact received by the player. The additional parts that we add to the player's uniform will monitor the most vital parts of the body, including the head/neck, lower back, and shoulder areas, and will constantly measure the force of impact caused during each collision in which the player is involved. If a collision registers a force in Newtons that is beyond what is safe, an alert will be sent to coaches and staff on the sideline, bringing attention to the afflicted player. Our product has the potential to identify concussions and serious injuries as soon as they appear, allowing coaches to step in and prevent further damage to their players. The hardware included in the design will be a Raspberry Pi 3 Model B which will collect the data obtained from the sensors and will transmit that data to the cloud. The Amazon Web Services Simple Queue Service (AWS SQS) will be implemented on the backend in a first-in-first-out priority. A front-end application will be developed that takes this information and displays it in a GUI that the coaching staff will be able view the data immediately. The estimated cost of the parts used is \$212.72, with the most expensive item being the load sensors, as well as the cloud services being provided by Amazon monthly. The cost of labor per unit is \$283.01. The proposed selling cost will be \$800 per unit.

# Measured Accumulative Underlying Real-time Impact Endo-skeleton

## 1. Introduction

The football community has a dire problem that has beleaguered it since its inception in 1869. The human body sustains permanent damage from participation in the sport, and there are no organizations that have used modern technology to make the sport as safe as possible for the players. To remedy this issue, our senior design team (Team Newtonian) has begun designing a full body suit to detect heavy collisions that may result in concussion or serious injury. We have titled our product M.A.U.R.I.C.E (Measured Accumulative Underlying Real-Time Impact Endo-Skeleton). Maurice will be a proof of concept product that will transform already existing padding made by companies such as Riddell and Schutt and transform them into data hubs capable of recording every hit that a player withstands during a game. This data will be sent to an application where coaches can view and analyze the data, making prompt decisions on the health of each player on the team.

### 1.1. Objective

The overall objective of this project is to provide coaches and training staff with quantitative data on the current health of their players on the field by recording the amount of force a player has withstood over the duration of the game. Rather than keeping track of the entire athlete's body, our design will only monitor the most vital areas, namely the lower back, and neck area. The data obtained will then be sent to the coaching staff via an application for immediate feedback. The project is a portion of a much larger design in which the ideal scenario would be to eventually develop a product that is able to monitor a majority of a player's body and provide a wider range of medical data, such as heartrate, attained speed, precision of routes, etc.

## **1.2. Motivation**

The motivation behind this project is the immediate health, as well as the long-term quality of life that students go on to live after football. While concussions have been at the forefront of the debate on player safety, the general effects of the game overall on the body is largely overlooked. The extensive amount of pain that players sustain has largely been blamed on the epidemic of painkiller abuse among professionals and students alike. Earlier this year in an interview with Fox News, former Ohio State University football player Shane Olivea revealed that at one point he was taking over a hundred Vicodin pills a day. Furthermore, the National Football League (NFL) has been accused of handing out pain pills like candy. Initially, this product will be intended for college athletes who, unlike professionals, are not paid for their sacrifices on the field. Currently, there are no products in use at any level that provides the functionality that we look to provide in our product. Companies such as Riddell have dedicated funds to technology for changes in the materials being used in the padding and helmets, however, as of yet there are no products that are used by the NCAA or NFL that delivers data on the health of a player's entire body in an application. Our product will not be launched as a cost-effective product, but as a life effective product. Currently, the NFL only carries former players on their corporate health insurance plan for up to five years after a player has retired, and this does not apply to players who were in the NFL for less than three years. Considering the average player's career only lasts for 3.9 years, there are many who will never qualify for the NFL's retirement coverage altogether. Colleges do not offer additional insurance beyond the student's eligibility at all. This is problematic for any participant in the sport as the effects of back and knee injuries can linger long beyond the grace period.

### **1.3. Background**

Key building blocks to ensuring the success of this project will lie in the transmission of recorded data from the sensors to the application. Not only does this transmission have to complete, but it must do so within the time the average college football play lasts, which is 6.07 seconds. The reason behind this number is that it is imperative that the training staffs are aware of the player's injuries before they attempt to assist him off the field, lest they risk causing additional damage by improperly handling an injured player.

In recent years, Riddell has partnered with the Virginia Institute of Technology to improve the design of their helmets and padding, reducing the number of concussions using their Riddell Flex helmet. However, Riddell has not pushed products with sensors that are built into the padding to the NCAA or NFL, largely due to the significant cost that it would impose as well as the reduction of mobility. This same issue will be something that will be challenging for our product. Our MAURICE system will include the following features:

## **2. Project Description and Goals**

The goal of this product is to increase player safety and longevity by providing real-time data on the force withstood over the course of a football game. To accomplish this, a Raspberry Pi 3 will be used to control the sensors and obtain the data. The pi will then access the IP address of a cloud server where the data will be stored. The application will then download and refresh its data from the cloud and use this data to display information to the user.

Product Features:

- Database of player health
- Sensors measuring force withstood

- Application that displays visuals of data
- Cloud Storage
- Animated 2D skeleton with color coded injury diagnosis

The monitoring process begins at the sensors which record the force withstood based on measurements taken by an accelerometer and gyroscope. These sensors will feed their data into a Raspberry Pi 3, which will send the raw data to a cloud server, identifying the player that the data belongs to and subsequently storing it in the player's profile on the server. From this point, the front end of the application will process the data and convert it into a visual of the human body where fatigue and injury are indicated by a color-coded system in which severely stressed, and possibly injured portions of the body are shown in a dark, crimson hue. The core of the product will lie in the database which will hold the data on each individual player. This information will be pulled down from a cloud server, taking account pre-existing injuries, personal statistics such as height and weight, and the number of plays participated in. Despite the challenges, a basic, working prototype is the goal with the above functionality being the baseline. The tablets that will be used to run the application will not have access to the internet like the Surface Pro's that the NFL uses on the sidelines. Instead, a mobile phone will be used as a hotspot, broadcasting internet throughout the testing site.

### **3. Technical Specifications**

The proposed product is required to seamlessly communicate between the on-body device and the user-interfaced endpoint on milli-seconds time scale, for approximately 150 MAURICE units. Within this time-span, sensory data that is periodically collected by the dedicated microcontroller is sent to the cloud services for processing and storing and` pushed to the user's web-app for analytics display. The system will consist of an accelerometer, optical heart rate, force sensitive resistor to collect impact



and force data. The prototyped system will also consist of a Raspberry Pi 3 Model B, an internet capable computer device (Laptop and/or tablet), and a suite of Amazon Web Services.

### **3.1. Raspberry Pi 3 Model B**

Processor	<ul style="list-style-type: none"> <li>• Quad Core 1.2GHz Broadcom BCM2837 64bit CPU</li> </ul>
Memory	<ul style="list-style-type: none"> <li>• 1GB RAM</li> </ul>
Connectivity	<ul style="list-style-type: none"> <li>• BCM43438 wireless LAN and Bluetooth Low Energy (BLE) on board</li> </ul>
Storage	<ul style="list-style-type: none"> <li>• Micro SD port for loading your operating system and storing data</li> <li>• Up to 16GB External SD storage</li> </ul>
Ports and Pins	<ul style="list-style-type: none"> <li>• 40-pin extended GPIO</li> <li>• 4 USB 2 ports</li> <li>• 4 Pole stereo output and composite video port</li> <li>• Full size HDMI</li> <li>• CSI camera port for connecting a Raspberry Pi camera</li> <li>• DSI display port for connecting a Raspberry Pi touchscreen display</li> </ul>
Power	<ul style="list-style-type: none"> <li>• Micro USB power supply (2.1A)</li> </ul>

### **3.2. Concussion detection sensor (Accelerometer)**

Acceleration (G Force)	<ul style="list-style-type: none"> <li>• 0 to 200 Gs (1g = 9.8 m/s)</li> </ul>
Sensitivity	<ul style="list-style-type: none"> <li>• 98 mg/digit @ (+-200 g)</li> </ul>
Operating Temperature	<ul style="list-style-type: none"> <li>• +85 °C Max</li> </ul>

### **3.3. Impact Detection (Load Cell)**

Force	<ul style="list-style-type: none"> <li>• 0 to 200 Kg</li> </ul>
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Sensitivity	<ul style="list-style-type: none"> <li>• 76 mg/digit @ (+-200 Kg)</li> </ul>
Operating Temperature Range	<ul style="list-style-type: none"> <li>• -20 to 60 °C</li> </ul>

### 3.4. Pressure detection (Flexi-Force sensor)

Maximum Force	<ul style="list-style-type: none"> <li>• 445 N (100 lbs)</li> </ul>
Sensing Area	<ul style="list-style-type: none"> <li>• 9.53 mm</li> </ul>
Response Time	<ul style="list-style-type: none"> <li>• &lt; 5 <math>\mu</math>sec</li> </ul>

### 3.5. Heart Rate detection

Range Pulse	<ul style="list-style-type: none"> <li>• 0 to 200 bpm</li> </ul>
Max. Sampling Rate	<ul style="list-style-type: none"> <li>• 100 samples/sec</li> </ul>
Range Waveform	<ul style="list-style-type: none"> <li>• 0 to 5 V</li> </ul>

### 3.6. Cloud

Queue	<ul style="list-style-type: none"> <li>• AWS Simple Queue Service (FIFO)</li> </ul>
Server	<ul style="list-style-type: none"> <li>• AWS Lambda</li> <li>• AWS Elastic Compute Cloud</li> </ul>
Database	<ul style="list-style-type: none"> <li>• DynamoDB (NoSQL) database</li> </ul>

### 3.7. ADC

Channels	<ul style="list-style-type: none"> <li>• 10 bit sampling in addition to additional 8 channels</li> </ul>
Sampling Rate	<ul style="list-style-type: none"> <li>• Max 50k HZ</li> </ul>
Communication Protocols	<ul style="list-style-type: none"> <li>• I<sup>2</sup>C and SPI channels</li> </ul>

### 3.8. Dashboard (Web-app)

Frontend Language(s)	<ul style="list-style-type: none"><li>• HTML/CSS</li><li>• JavaScript</li></ul>
Backend Languages(s)	<ul style="list-style-type: none"><li>• Python</li><li>• C#</li></ul>
Framework	<ul style="list-style-type: none"><li>• Flask (Python)</li></ul>

## 4. Design Approach and Details

### 4.1. Design Approach

#### 4.1.1. *System Overview*

There are three main components to MAURICE: the hardware within the suit, the cloud, and the web application. Figure 1. shows the block diagram of the overall system.

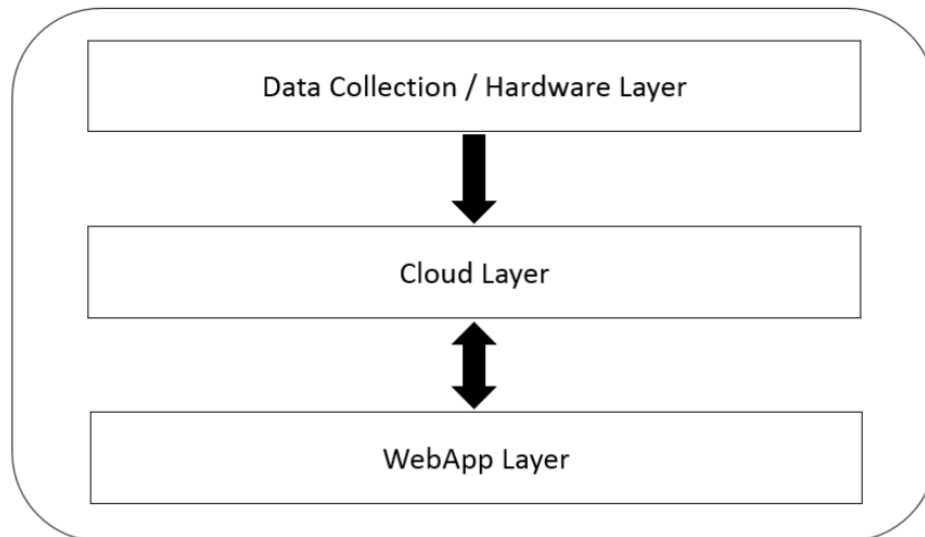


Figure 1. A block diagram of the MAURICE system

The hardware side consists of sensors, a microcontroller, and a battery. The microcontroller receives the measured data from the sensors and transmits them to the cloud layer through its Wi-Fi chip.

The Cloud layer processes the received data from the hardware side; it stores the data into the data base, regressively analyzes the data, and transmits to the web application server. Lastly, the web application is an intelligent Graphical User Interface (GUI), which represents the health status of the player wearing the corresponding suit by 2-D image of a human body, graphs, and color scales.

#### 4.1.2. Hardware

The hardware layer mainly includes sensors, which are embedded into the corresponding parts of the suit and a microcontroller and a power source located at the back of the suit. Figure 2. Illustrates communication and data flow between each hardware device.

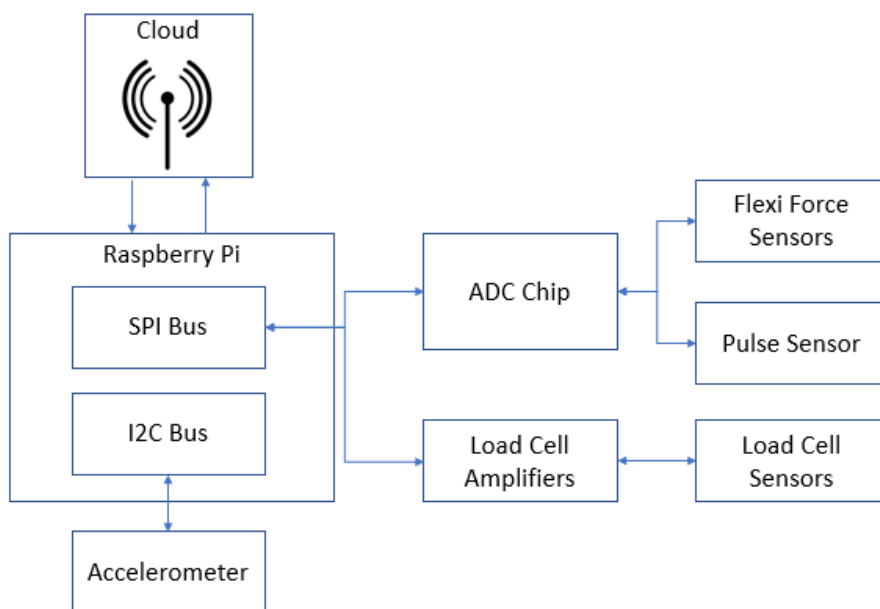


Figure 2. A block diagram of the hardware communicating system.

##### 4.1.2.1. Sensors

There are three types of sensors that are going incorporated into the suit; an impact sensor, concussion sensor, and heartbeat sensor. The impact sensor is a semi-conductor device, which changes its resistance corresponding to the magnitude of exerted impact [1]. It will measure the magnitude of impact a body part experiences in terms of voltage and current. is an analog sensor that e specifically added to the player’s helmet; it is essentially an accelerometer, which measures the shock exerted to the

helmet in terms of an acceleration. Studies show mild concussions begin to occur approximately at 100g of exerted force on a player's head and severe concussions at about 150g. The sensor implemented on the helmet should be capable of measuring above this threshold [2]. Finally, there is a heartrate sensor, that measures pulse based on optical power variation as light is scattered during its' path through the blood as the blood flow changes during a heart cycle [3]. For the communication side, because a pulse and flexi force sensors are analog sensors, we use an additional ADC (Analog-To-Digital Converter) chip to sample and transmit the binary data to Raspberry Pi. Impact sensors are also analog devices, but they are always used with the amplifier chips, to prevent the effect of noise upon the low gain, which also does the digital sampling. Last, accelerometer has digital sampling feature in its' own, so it does not require an additional ADC device. All the sensors are embedded into the corresponding part of the suite and helmet and send the data to the Raspberry Pi, which is located at the back part of the suite with the battery.

#### ***4.1.2.2. Microcontroller***

The measured data from the sensors will be collected by a Raspberry Pi. The Raspberry Pi is a small, single board computer that includes a variety of features such as GPIO, networking, and a real-time clock. Its' function is to receive measured data from the sensors altogether by threading and transmit it to a cloud server using a built in Wi-Fi module [4]. The Raspberry Pi includes both I<sup>2</sup>C and SPI bus, and we are using those protocols to communicate with the corresponding sensors. Both I<sup>2</sup>C and SPI protocols are similar in a sense that Raspberry Pi is the master, which does a main job of transmitting and receiving data from the slaves, the other devices, but I<sup>2</sup>C bus communicates with other devices based on their addresses while SPI bus uses sampling clock, input, output, and SS signal line, which sends the selecting signal to choose the devices to communicate. While accelerometer uses I<sup>2</sup>C protocol as a communication bus, all other sensors interacts with the Pi through the SPI bus and each of those devices

is selected by SPI bus by the SS and communicates with the Pi one at a time. The Raspberry Pi also can do a lot more in terms of computation than what is needed for this project. Despite this, we are using it for our prototype since it is a proven controller that can handle this task with limited complications and increased simplicity. If MAURICE were to be used in a typical application i.e. needing mass manufacturing, then a low-cost microcontroller would be used. The microcontroller, and a power supply will be mounted on the back of the player's suit. It will transmit real time sensor data at a certain sampling frequency based on the logic of the interrupt-based programming. This rule will be applied to not only the microcontroller, but also the cloud and web application layers to operate the entire system in real-time. Lastly, 8GB of micro SD card is used as the memory device of the Pi, and this offers enough amount of computation storage until the power supply will run out.

#### **4.1.3. Cloud**

The concept behind cloud computing is using a repetitive network of remote servers hosted and accessible via the internet to store, manage, and process data. The use of cloud computing has eliminated the need for local servers and high performance and capacity computers to run computationally intensive applications and programs. Cloud computing offers a plethora of computing solutions like web-based storage, server-side application delivery and consumption, and much more [5]. In this project, the key role of the cloud layer is to receive data produced from end-points (suit, web app) to be processed for consumption by various ports. One of the consumer of the processed data is the dedicated dashboard on the web app.

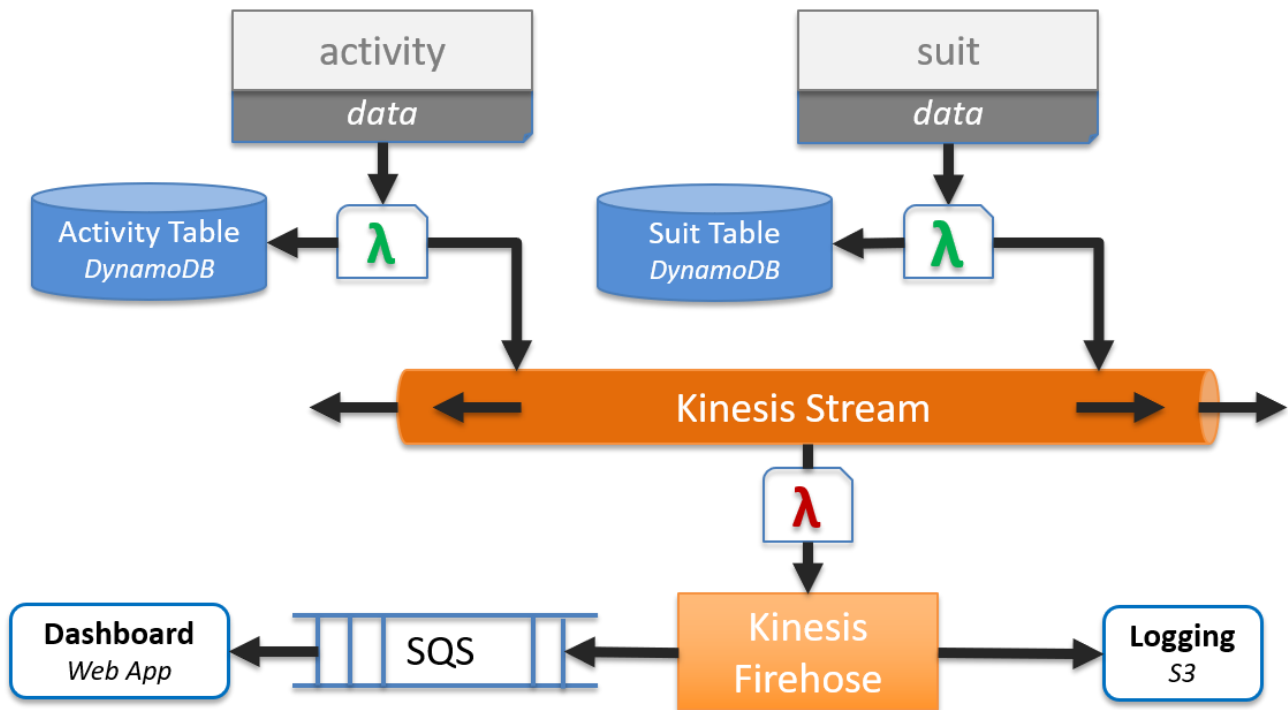


Figure 3. Implemented architecture of the cloud layer using micro-services

#### 4.1.3.1. Communication Layer

The design approach for the cloud layer is as illustrated in Figure 3. The suit and web app endpoints as source of production produce activity and suit data packets sent to the cloud via an established Application Programming Interface (API). Using a micro-service approach, the various services are modularized to prevent creating direct dependencies of the various producers and consumers. The micro-services implemented were the *Activity* micro-service, the *Dashboard* micro-service, and the *Suit* micro-service. The API Gateway as an AWS service serves as the established gateway, which implements resources that maps to the different micro-services. The resources are thereafter mapped to an AWS Lambda function that effectively processes the received data, according to the desired HTTP Create-Read-Update-Delete (CRUD) method protocols.

#### **4.1.3.2. Data Processing**

For instance, taking a closer exploring the activity micro-service in Figure 3, the published data is taken in by the relative lambda function that transformed the received data into an *activity* data packet. The transformed activity data packet is published to the *Activity Table*, which is implemented as a NoSQL data table. The data table is an instance of the AWS DynamoDB service. Further, the transformed activity data is also pushed into a real-time serving data stream (an instance of the AWS Kinesis Stream). The data published to the stream have a life-span to which they are retained in the stream and can be consumed. This process allows multiple consumers to consume the same data, which can be useful for having multiple authorized dashboard view the data simultaneously, in real-time. The data stream was implemented with a single shard to stay within the allocated budget, however, it should be noted that several shards ought to be created to have higher performance from the serving data that was published to the stream.

After having published the transformed activity data unto the data stream, another lambda function is activated to further process the data to be ready for consumption. The approach of consuming the data utilize instances of AWS Kinesis Firehose. With one instance of the firehose, the transformed activity data packet on the stream is further transformed and pushed unto a First-In-First-Out (FIFO) queue as an instance of AWS SQS service. It is from the Sequential Queuing Service that the dashboard micro-service consumes relevant data to be rendered on the dedicated GUI web app, in near real-time. Another instance of the firehose consumes from the data stream to create generate and store logs on cloud storage, using the AWS Simple Storage Service (S3).

#### **4.1.4. Graphical User Interface**

The GUI layer collects the data of each player from the cloud layer and represents it visually by using a 2D image of a human body, graphs, and numerical values. Figure 4. illustrates a view of a single player and his or her data on the GUI.





Figure 4. The GUI interface to represent the processed data

The left top side of the screen contains live graphs showing real time impact data of the head, torso, and arms measured by impact sensors attached to the suit. The left bottom side of the screen displays a gauge representing the measured pulse of the player. Above the body image, a number corresponding to the concussion (acceleration) rate and an associated safety scale is visible. While the impact and heart rate graphs represent the measured sensor values over time, the concussion rate is determined by the accumulated concussion sensor values over time. The 2D image of a human body located on the right of the screen illustrates the degree of injury of each body part by color. A player's body condition at the beginning of the match is represented by white, and the corresponding body part becomes a shade of yellow and red as more damage is accumulated on a specific part of the body as the match progresses. The health status of the player is determined by the overall injury rate of the player's body, and it will be in the box below the 2D rendering of the human body as text.

## 4.2. Codes and Standards

The handling of data pertaining to an individual is characterized as personal and sensitive. When collecting this data from a user that wears a MAURICE suit, the data is required to follow the NIST800-53 (Technical Access Control) data security standards. In abiding to the NIST800-53 standards, the transmission, storage, accessibility, active account management and role authorizations must be established. The transmission of data that is deemed personal should follow the Technical Access Control AC-1 Access Control Policy and Procedures P1 [6]. More notably, the data that is to be collected relates to the user's health information that demands maintaining government-controlled standards in the acquisition, transmission, storage, and manipulation of collected data [7]. The collected data that is to be transmitted will be sent over a secure and encrypted wireless communication network, that uses a *Private-Public key hashing* technique to validate data. Making use of Amazon Web Services solutions, the security of the data is in-built into the services, with the User Roles methodology. On the consumption side of the data, User-Password authentication will be used to ensure authorized access to sensitive data.

Since we will be relying on Wi-Fi communication to connect the data collection points i.e. the smart suit to the cloud we will need to follow a widely used Wi-Fi standard. IEEE 802.11 is a wireless-networking standard that uses multiple antennas to increase data rates [8]. Almost every Wi-Fi access point today is compatible with this standard. We need to use hardware that would also follow this standard on our suit like the Raspberry Pi single board computer.

## 4.3. Constraints, Alternatives, and Tradeoffs

### 4.3.1. *Durability*

The durability of the design proved to exceed initial expectations. During the senior design expo, Aaron simulated real game activity in which he lined up against Buzz, and the two blocked each other for

five seconds. Despite the contact, the suit remained intact and continued to measure readings. While the suit could withstand some moderate contact over a short matter of time, the current housing is still plastic and will quickly buckle if it collides with the metal helmets, shoulder pads, etc.

#### ***4.3.2. Power Consumption***

During testing, a 16,000 mAh battery was used to power the suit. In our demonstrations, the battery lasted over long periods of time. After a testing session of two hours, the battery only decreased in charge by 8%. While power consumption was not an issue for the project, one problem that will be an area of concern going forward will be the heat that is emanated from the Pi during gameplay. In one instance, the Pi overheated from use, and the subsequently shut off soon after. To prevent this from occurring in future runs, the software was modified to rest during times when movement was not detected to avoid using power on calculating garbage values.

#### ***4.3.2 Size***

The overall size that the modifications to the tradition suit was 7" x 11" x 3" which comes from the housing for all the parts that were needed to maintain the Pi. This area can be largely reduced with the redesign of the packaging by creating a PCB that routes the interconnects rather than using a traditional breadboard that relies on adhesives to stay mounted in placed.

## **5. Schedule, Tasks, and Milestones**

To guide the group in setting milestones and managing our time, the group created a detailed time line to describe the estimated time for each task our project requires. As discussed during lecture, a GANTT chart is used to outline and schedule all tasks needed for this project from beginning to end (Appendix). The GANTT chart estimates the duration of each task based its difficulty. Each task is assigned to the team member(s) most suited to complete it, except for the website, which everyone will contribute to. For example, the Prototype Component Board (PCD) assembly and design task will be taken by the team members majoring in Electrical Engineering or Computer Engineering with a hardware focus, while the GUI implementation and backend design will be assigned by those who specialize in software. The more time-consuming processes are expanded upon in the PERT chart. This chart breaks down sub tasks comprising the critical path tasks. To minimize the risk of spending more time then we have allotted on these tasks, our group is prepared to "borrow" members from our internal teams who have experience on the tasks to expedite the process.

## **6. Project Demonstration**

The system was demonstrated in both a non-stress environmental as well as a simulated game time scenario. Under normal testing, a participant would come forward and punch one, or both of the two load sensors placed in the chest. After the initial shock wave of had subsided, the data was transmitted to the Raspberry Pi and then displayed on a monitor. During the demonstration in McCammish Pavillion there were hundreds of devices connected to the Wi-Fi simultaneously which caused significant delays in the latency. On average, lags were approximately 13 seconds.

1. The test subject fully wears the football body protective gear and helmet
2. The computer on the suit is turned on and set up

3. A varying range of impact applied to the various sensory areas on the suit
4. Observe the correlating information rendered on the web app GUI

This process will be repeated as needed to highlight impact detection, as well as MAURICE's capabilities of assessing compound impacts to specific body parts. Furthermore, the time delay in transmitting a sensed impact to rendering is measured and monitored. Other demonstrations will be performed to test specific aspects of the system hardware.

From conducted tests, the time taken to send sensory data from suit to cloud was approximately *400 – 500 milliseconds*. Once the data is on the cloud, the processing, transformation, and logging takes approximately *790 milliseconds*. To follow fully on the data path, it takes approximately *200 – 300 milliseconds* from query to delivery from the web app. As an end-to-end time, a data packet took *1290-1590 milliseconds* from publication to rendered consumption.

## **6.1. Impact Measurement**

Impact detection was demonstrated by subjecting the upper chest of the player wearing the pads to a series of open fist thrusts, pushes, and punches. Within 500-700 milliseconds the amount of force detected by the load sensors were displayed on the server side using the processing power of the raspberry pi. On the client side, impact results took much longer to register, in some cases taking up to 15 seconds to become available on the web application. This delay was likely a result of the large load on the wifi as a result of hundreds of students trying to connect simultaneously, and we do not expect this to continue to be an issue. Under normal loads on GT wifi, the latency for the application was closer to 3-5 seconds.

## **6.2. Heart Rate**

The results of the heart rate monitor were less than stellar in our testing. The issue that was prevalent was that the heart rate sensor that was used in this project must always have direct contact with the finger tips. This is because the wavelength of the light that is emitted from the LED is not strong enough to penetrate any other portion of the body. The issue with this is it is not realistic to run a wire from the Raspberry Pi to which is located on the lower back, down the arms and to the hands. A solution that was proposed for future development to add this feature was to have wireless communication on a simple 2.4 GHz radio frequency that can send the recorded beats per minute from the sensor to the Pi. Another potential solution is the development of a device similar to the commercial Fitbit trackers which can monitor heart and then send that data to a mobile device via Bluetooth. The addition of the prototype will cost an additional \$75 in future iterations.

## **6.3. Acceleration**

Acceleration was tested by the accelerometer implanted within the front crown of helmet. Four wires were used to connect the part to power and ground, as well as SCL and SDA data ports. The values of the acceleration were then displayed in the web application and if a sudden change above 10Gs occurred, indicating the likely probability of a concussion.

# **7. Marketing and Cost Analysis**

## **7.1. Marketing Analysis**

Concussions have been a topic of great concern in football, and this has motivated a demand for advancements in technology that prevent these injuries. There currently exist multiple products that track impacts to the head and relay the information to a mobile application. Of these products, two

particular products stand out – *Riddell InSite* and *Shockbox*. Taking a closer look into the aforementioned products:

***Riddell InSite:***

*The Riddell Insite system is composed of sensors positioned inside player helmets to monitor impacts received during play, while computing the metrics associated with said impact (e.g. location, linear and rotational acceleration). High magnitude impact sends a detailed alert to coaches, detailing the impact and player information [2]. The Insite system sells for \$1000, and includes software to track each player registered in its database [3].*

***Shockbox:***

*Shockbox Helmet Sensors offer a portable sensor that can be placed on athletic helmets, as opposed to sensors that are embedded in the internal padding of a helmet. Each sensor interfaces with a mobile phone application through Bluetooth communication, sending alerts when a sensor detects an impact over its set threshold.*

Our product has multiple capabilities including those from both products: integrated suit sensors, website, mobile application, and cloud services. These products exist as external attachments to a sports' helmet while our technology is embedded within players' equipment. This allows for more accurate measurements. More notably, these products have little to no focus on other parts of the body. The MAURICE system tracks the head, limbs, and the chest area allowing for a larger number of measurement points and better critical decisions made by the application.

## 7.2 Cost Analysis

### 7.1.1. Cost of Components

Raspberry Pi 3	\$ 39.95
Sensor – Heart rate/pulse	\$ 24.99
Sensor – Accelerometer (H3LIS331DLTR)	\$ 9.95
Sensor – Load cell	\$56.95
Sensor – Flexi force Sensor	\$ 19.95
ADC for Pulse Sensor and Flexi Force Sensor	\$ 14.99
Amplifier w/ ADC for Load cell	9.95
Power source – External battery pack	\$ 35.99
<b><i>Total Component Costs</i></b>	<b>\$212.72</b>

### 7.1.2 Cost of Labor (R &D)

Team members	6
Engineering Salary per person	\$ 60,000 /year or \$ 5000 /month
Project timeline	5 months
<b><i>Total labor cost</i></b>	<b>\$150,000.00</b>

### 7.1.3 Cost of Production

MAURICE unit	\$ 212.72
Estimated units sold (10 NFL teams of 53 players each)	530 units
Cost of labor for each unit (Labor cost for 5 months ÷ Number of units)	\$ 283.01
<b><i>Total production cost</i></b>	<b>\$495.7 / unit</b>



### 7.1.4 Profitability

Projected Sales	530 Units
Selling Price	\$800 / unit
Profit per unit (Selling price – Cost of Production)	\$ 304.3
<b>Total Profit for 5 months</b>	<b>\$161,279.00</b>

### 7.1.5 Maintenance Costs (to the customer)

Cloud Service (10 or less concurrent users): <ul style="list-style-type: none"><li>• Web Servers X 3 – (2 Cores, 8GB RAM, 500 GB HDD)</li><li>• App Servers X 2 – (4 Virtual Cores, 16 GB RAM, 30 GB HDD, 15 GB Data transfer)</li></ul>	\$ 63.15 (per month, per NLF team)
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## 8. Conclusion

The result of the project yielded success in the areas of basic functionality which included impact detection as well as detection of rapid deceleration which can often indicate possible concussions. After subjecting the suit to dozens of consecutive hits, there was near perfect detection of impact in the chest area ranging from the sternum to the collarbone. One particular edge case that occurred twice was that occasionally the duration of the impact was shorter than the sampling frequency of the raspberry pi. To avoid killing the battery too quickly, the sampling frequency of the load sensors were decreased, but because of this, it makes it possible for short impacts to transpire before the next sampling occurs. Some of the shortcomings of the design was in the fact that we used a breadboard rather than manufacturing a PCB. By using a PCB, efficiency and space could have been improved. The helmet did function as expected in that it measured the deceleration of the brain, however, this was only effective in measuring head on collisions and not torsion which could occur in hits where the defender collides with the offensive players at varying angles.

The one component that will be removed due to its lack of functionality on the field are the flex force sensors. Like the heart rate sensor, the flexi force sensor requires constant contact with the skin, which causes it to have some of the same issues as the heart rate sensor. A more pressing problem is that the flexi force sensing element only accounts for approximately 15% of the total area that the sensor housing. During testing if pressure was not applied directly to the location where the sensing element was located then no impact was detected. For this reason, we have decided it is best to explore other options for analyzing soft tissue injuries.

### Leadership Roles

The team was split into two different teams, each person having their own leadership role. On the software side:

Olatide Omojaro was in charge of the cloud computing. He handled the storing of data from the Raspberry Pi to the cloud on an AWS server.

Daniel Albuquerque handled the hardware software which involved tuning the accelerometer, pulse sensor, and flexi sensor. Also manufactured some of the aftermarket enclosures that were used to house the components within the suit.

Kevin Webb: Webmaster and architect of the application that displayed the data being collected from the suit. Completed the client-side GUI which was what the end users got to see and the Expo as well the the team website that holds additional information on the group members and project ideas.

Aaron Thurston: Hardware Lead: completed low level software development in Python on the Raspberry Pi and regulated I2C ports for rapid data transfer as well as the conversion of binary data in a bitstream to user readable data.

Jiwon Lee: Hardware engineer. Crafted many of the interconnections necessary for powering and transporting data from the sensors to the Pi.

Drevon Taylor: Expo Leader and responsible for the remodeling current football equipment already on the market, gutting, the design, and then crafting new padding, plating, and connections between the helmet and raspberry Pi. Also created powerpoint presentations for demo.

## 9. References

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# Appendix

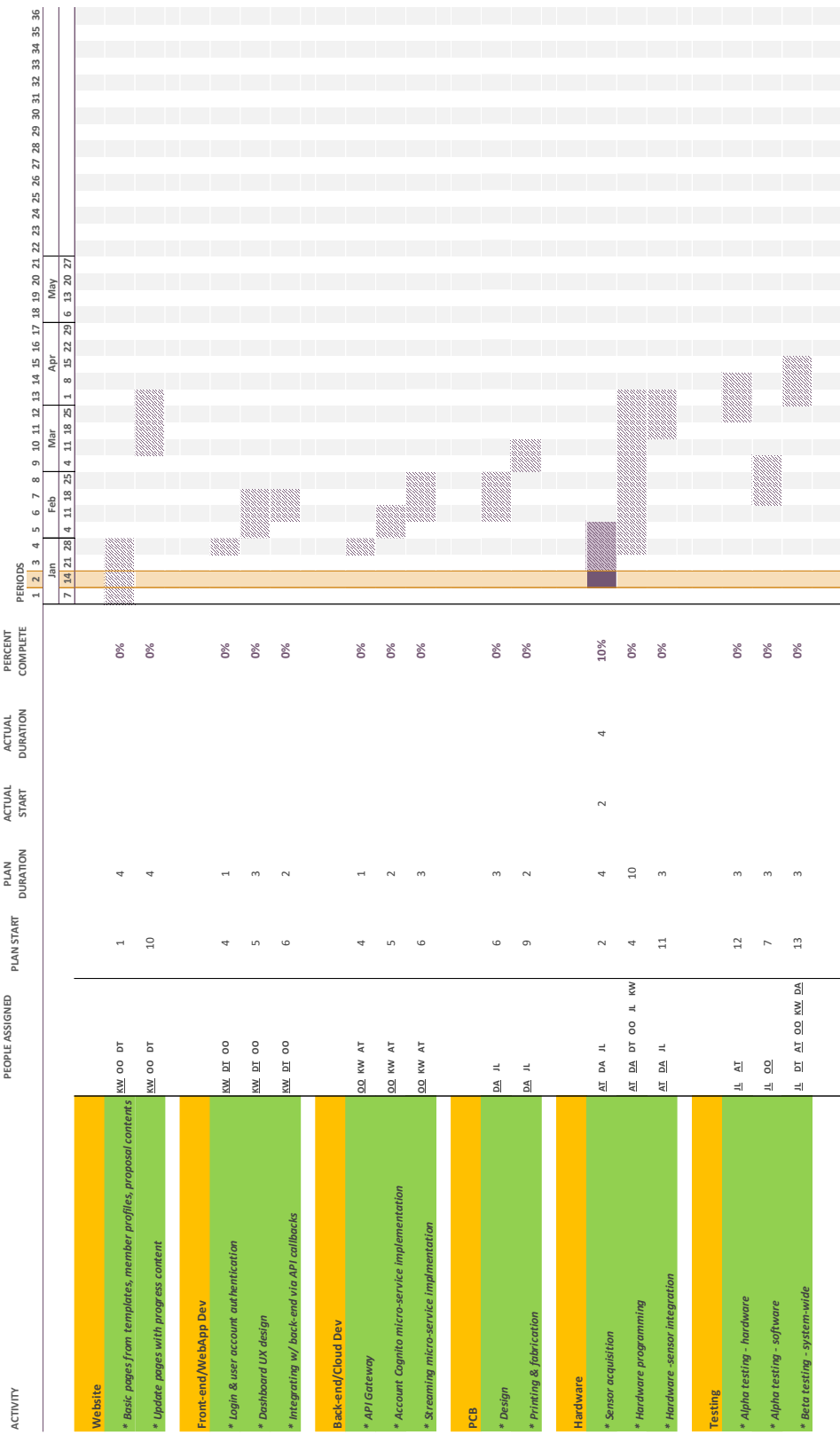
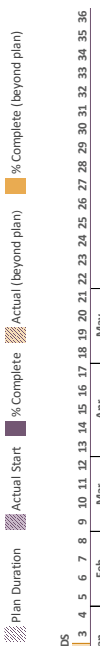
## A. GANTT Chart

### Newtonian's MAURICE Project Planner

Select a period to highlight at right. A legend describing the charting follows.

Period Highlight: 2

Plan Duration Actual Start Actual (beyond plan) % Complete (beyond plan)



<i>Team-Member</i>	<i>Initials</i>	<i>Team(s) Led</i>	<i>Other Obligation(s)</i>
Aaron Thurston	<b>AT</b>	Hardware	Back-end
			Hardware
			Testing
Daniel Albuquerque	<b>DA</b>	PCB	Website
		Hardware	Testing
Dre Taylor	<b>DT</b>	Front-end	Website
		Weekly Summary	Testing
Jiwon Lee	<b>JL</b>	Testing	PCB
			Hardware
Kevin Webb	<b>KW</b>	Website	Back-end
		Front-end	Testing
		Design Book check	
Olatide Omojaro	<b>OO</b>	Back-end	Website
			Front-end
			Hardware

## B. PERT Chart

